1	Approaches to Account for Colon Absorption in
2	Physiologically Based Biopharmaceutics
3	Modeling of Extended Release Drug Products
4	Harshad Jadhav <sup>1,2</sup> , Patrick Augustijns <sup>2</sup> , Christer Tannergren <sup>1, *</sup>
5	<sup>1</sup> Oral Product Development, Pharmaceutical Technology & Development, Operations,
6	AstraZeneca Gothenburg, S-431 83 Mölndal, Sweden
7	<sup>2</sup> Department of Pharmaceutical and Pharmacological Sciences, KU Leuven, ON2 Herestraat
8	49, 3000 Leuven, Belgium
9	
10	KEYWORDS: Physiologically based biopharmaceutics modeling; PBBM; PBPK; Extended
11	release; colon absorption; regulatory applications
12	
13	ABSTRACT
14	The rate and extent of colon absorption are important determinants of the in vivo performance
15	of extended release (ER) drug products. The ability to appropriately predict this at different
16	stages of development using mechanistic physiologically based biopharmaceutics modeling
17	(PBBM) is highly desirable. This investigation aimed to evaluate the prediction performance
18	of three different approaches to account for colon absorption in predictions of the in vivo

19 performance of ER drug product variants with different *in vitro* release profiles. This was done 20 by mechanistic predictions of the absorption and plasma exposure of the ER drug products using GastroPlus<sup>®</sup> and GI-Sim for five drugs with different degrees of colon absorption 21 22 limitations in humans. Colon absorption was accounted for in the predictions using three 23 different approaches: (1) by an *a priori* approach using the default colon models, (2) by fitting 24 the colon absorption scaling factors to the observed plasma concentration-time profiles after 25 direct administration to the colon in humans or (3) from the ER drug product variant with the 26 slowest in vitro release profile. The prediction performance was evaluated based on the 27 percentage prediction error and the average absolute prediction error (AAPE). Two levels of 28 acceptance criteria corresponding to highly accurate (AAPE  $\leq 20\%$ ) and accurate (AAPE 20-29 50%) predictions were defined prior to the evaluation. For the *a priori* approach, the relative 30 bioavailability (Frel), AUC<sub>0-t</sub>, and C<sub>max</sub> of the ER drug product variants for the low to medium colon absorption limitation risk drugs was accurately predicted with an AAPE range of 11-31 53% and 8-59% for GastroPlus® and GI-Sim, respectively. However, the prediction 32 33 performance was poor for the high colon absorption limitation risk drugs. Moreover, 34 accounting for the human regional colon absorption data in the models did not improve the 35 prediction performance. In contrast, using the colon absorption scaling factors derived from the slowest ER variant significantly improved the prediction performance regardless of colon 36 37 absorption limitation, with a majority of the predictions meeting the high accuracy criteria. For the slowest ER approach, the AAPE range was 5-24% and 5-32% for GastroPlus<sup>®</sup> and GI-Sim, 38 39 respectively, excluding the low permeability drug. In conclusion, the *a priori* PBBM can be 40 used during candidate selection and early product design to predict the *in vivo* performance of 41 ER drug products for low to medium colon absorption limitation risk drugs with sufficient 42 accuracy. The results also indicate a limited value in performing human regional absorption 43 studies where the drug is administered to the colon as a bolus to support PBBM development for ER drug products. Instead, by performing an early streamlined relative bioavailability study
with the slowest relevant ER *in vitro* release profile, a highly accurate PBBM suitable for ER
predictions for commercial and regulatory applications can be developed, except for
permeability-limited drugs.

### 48 INTRODUCTION

49 Extended-release (ER) drug products may offer several benefits compared to immediaterelease (IR) counterparts, such as minimizing side effects associated with peak plasma 50 51 concentrations, delivering drugs to specific locations in the gastrointestinal tract, reducing dosing frequency, and ultimately improving patient compliance<sup>1-5</sup>. This is achieved by 52 designing the ER drug product to release the drug content over an extended period, often 53 54 exceeding the small intestinal transit time. Consequently, the performance of an ER drug 55 product also relies on sufficient drug release and absorption in the colon. Therefore, accurate 56 assessment and predictions of colon absorption are crucial for the successful development of ER drug products<sup>1, 6, 7</sup>. However, the colon presents challenges for drug absorption due to its 57 58 small surface area, tight junctions in the epithelial cell layer affecting permeability and 59 membrane transport, low water content, very low bile salts, and irregular motility pattern, which can restrict drug dissolution<sup>7-13</sup>. Furthermore, drugs may undergo bacteria-mediated 60 61 luminal degradation as well as bind to the solid/semisolid intracolonic contents, potentially hindering drug absorption<sup>14-16</sup>. Therefore, the current *in vitro* and *in vivo* methods focus on 62 assessing the rate and extent of colon absorption in humans<sup>17-23</sup>. Recently, the usefulness of 63 physiologically based biopharmaceutics modelling (PBBM) to predict human colon absorption 64 has been demonstrated<sup>24</sup>. However, it has not been evaluated how useful this is in predicting 65 the in vivo performance of ER drug products. PBBM, or physiologically based 66 67 pharmacokinetics modelling (PBPK) for biopharmaceutics applications, is increasingly being

used to guide oral drug product development<sup>25-39</sup>, and FDA has issued a draft guidance to 68 support the use of PBBM for regulatory submissions<sup>33</sup>. PBBM can be used throughout the drug 69 70 development process to optimize the *in vivo* performance of the drug product, enabling dose 71 optimization, risk assessment, and supporting regulatory decision-making. Several software packages, such as GastroPlus<sup>®</sup>, Simcyp<sup>®</sup>, PK-Sim<sup>®</sup>, and GI-Sim, are used to predict the *in vivo* 72 73 performance of a drug product. The majority of the PBBM applications have focused on 74 predicting the absorption after administration of IR drug products, where absorption 75 predominantly occurs in the proximal small intestine. Less emphasis has been put on predicting 76 the absorption of modified/extended-release (MR/ER) drug products, which pose additional 77 challenges due to the need for modeling regional intestinal differences in absorption, and it has 78 been stated that the prediction of colon absorption using PBBM is a current modeling and simulation capability gap<sup>26, 40, 41</sup>. To date, only a few investigations have been made on using 79 80 PBBM to predict the *in vivo* performance of ER drug products. Most of the applications have 81 been based on top-down approaches, where an *in vivo* understanding of the drug product was 82 known, and few investigations accounted for colon absorption by adjusting the colon physiology parameters<sup>8, 22, 25, 42, 43</sup>. In addition, there has been no systematic investigation of 83 84 the prediction performance for different approaches to account for colon absorption in PBBM of ER drug products for drugs with different risk levels of colon absorption limitations. 85 Therefore, this study aimed to evaluate the prediction capability of GastroPlus<sup>®</sup> and GI-Sim 86 87 for ER drug products where colon absorption was accounted for using three different 88 approaches: (1) by an *a priori* approach using the default colon models or (2) by fitting the 89 colon absorption scaling factors to the observed plasma concentration-time profiles from direct 90 human colon administration or (3) from ER drug product variants with the slowest in vitro 91 release profile. The prediction results were evaluated in relation to the assigned colon 92 absorption limitation risk.

# 94 MATERIALS AND METHODS

# 95 Model drug selection & dataset establishment

The model drugs in this study were selected based on the availability of colon absorption data from human regional absorption studies and *in vitro* release profiles for several ER drug product variants with corresponding human *in vivo* pharmacokinetic data together with a mechanistic understanding of the factors affecting their regional and colon absorption (**Table** 

100 **1**).

Parameter	Unit	Metoprolol <sup>44</sup>	Oxprenolol <sup>44</sup>	AZ2 <sup>44</sup>	AZ144	Ximelagatran <sup>44</sup>
Molecular weight	g/mol	267.36	265.34	250±5	500±5	429.5
LogD (pH)		1.74 (logP)	0.14 (7.4)	0.8 (6.7)	4.3 (7.4)	-1.3 (7.4)
рКа		9.18 (base)	9.5 (base)	10.7 & 7.18	3.05 (base)	2 (acid), 7 & 11.5
				(acid)		(base)
Solubility (pH)	mg/ml	43 (6.5)	15 (6)	0.06 (1.8)	0.007 (7.4)	215 (7)
Diffusion	10 <sup>-5</sup> ×cm <sup>2</sup> /s	0.8169	0.8203	0.8427	0.5704	0.6336
Drug particle density	g/ml	1.2	1.2	1.2	1.24	1.2
Particle radius	μm	25	25	25	5	25
Human jejunal Peff	10 <sup>-4</sup> ×cm/s	1.34	5.1	2.03	8.8	0.10
FPE	%	40.126	29.15	0	64	64
B:P		1.07	0.9	1	0.6	0.6
Fup	%	90	12	26	0.1	86
CL <sub>H</sub>	l/h/kg	0.552024	0.33731	0.16194	0.1569	0.02944
CL <sub>R</sub>	l/h/kg	0.061336	0	0	0.00008342	0.08256
Vc	l/kg	1.5304	0.22416	0.03808	0.174	0.134
k12	1/h	1.3633	9.0486	16.018	3.267	0.31624
k21	1/h	1.4717	5.9581	9.5998	0.84	0.11501
k13	1/h	20.639	0.31433	5.7453	0.373	0
k31	1/h	27.641	0.03505	1.1587	0.0142	0

101 **Table 1.** Drug-specific model input parameters used for the PBBM of the model drugs

102FPE- First pass extraction, B:P- blood to plasma ratio,  $F_{up}$ - fraction unbound in plasma,  $CL_{H}$ - hepatic clearance,103 $CL_{R}$ - renal clearance.

104

105 The selected drugs were categorized into low, medium, and high colon absorption limitation 106 risk based on the *in vitro* permeability and dose to solubility ratio. A drug is considered to be 107 highly permeable when the *in vitro* permeability is higher than that of a high permeability 108 marker, such as metoprolol or minoxidil, or when the permeability corresponds to a fraction absorbed in the colon (Fabs<sub>colon</sub>) of 85% or higher according to previously established *in vitro* apparent permeability ( $P_{app}$ )-Fabs<sub>colon</sub> correlation<sup>7, 44</sup>. The estimated dose to solubility ratio is based on the dose of non-solution formulations administered directly to the colon in the human regional absorption studies, in relation to the buffer solubility in the pH 6.3-6.8 range determined according to internal AstraZeneca best practice (**Table 2**)<sup>7</sup>.

- 115
- 116

Drug Permeability class Dose: solubility ratio Colon absorption risk (Limiting factor) High Metoprolol Low Low (-) High Oxprenolol Low Low (-) AZ2 High Medium (Solubility/Dissolution) Medium AZ1 High (Solubility/Dissolution) High High High (Permeability) Ximelagatran Low Medium

117 **Table 2.** Classification of the model drugs based on colon absorption limitation risk

118 All clinical data were gathered from previously published work or studies performed in-house 119 at AstraZeneca. The human effective permeability (Peff) for the model drugs used in the 120 predictions was either the measured clinical value or estimated using measured in vitro intrinsic 121 Caco-2 apparent permeability (Papp) values combined with a previously established Caco-2 Papp – human P<sub>eff</sub> correlation<sup>44-46</sup>. *In vitro* buffer solubility data combined with the pKa values were 122 123 used to establish a pH-solubility profile used in the predictions according to the Henderson-124 Hasselbalch equation (Table 1). The mean particle radius of 25 µm was used for drugs where particle size data were not available. In GastroPlus<sup>®</sup>, the default solubility (Sol) factor of 50 125 126 was used for all drugs<sup>44</sup>. It was assumed that no precipitation occurred *in vivo*, and the mean 127 precipitation time was adjusted accordingly<sup>44</sup>. All the pharmacokinetic/disposition parameters used in the model development were estimated by fitting the intravenous and/or oral solution 128 129 data to either two or three compartment pharmacokinetic models. The same pharmacokinetic parameters were used in each software during the predictions. For the prodrug ximelagatran, the disposition model was developed based on the appearance of the active drug in plasma after absorption<sup>47</sup>. The hepatic extraction ratio ( $E_H$ ) was either obtained directly from literature or estimated by **Equation (1)**<sup>48</sup>.

- 134
- 135

$$E_{\rm H} = \frac{CL_{\rm H}}{Q_{\rm H} \times B:P} \tag{1}$$

136

137 where Q<sub>H</sub> (1.5 L/min), CL<sub>H</sub> and B:P are the hepatic blood flow, hepatic clearance, and blood 138 to plasma ratio, respectively.  $CL_H$  was calculated by  $CL = CL_H + CL_R$ , where  $CL_R$  is the renal 139 clearance. The physicochemical, biopharmaceutics, and pharmacokinetic input parameters for 140 all drugs are summarized in **Table 1**. The *in vitro* dissolution profiles used in the modeling of 141 ER drug product variants were generated using discriminatory USP I or II methods, which all 142 were the established methods to support the development of each drug product<sup>44</sup>. In addition, 143 the *in vitro* dissolution method for oxprenolol was used to establish a relationship with *in vivo* drug release<sup>49</sup>. The ER drug product variants for the model drugs were categorized as fast, 144 145 medium, and slow based on the time to release 80% of the drug content *in vitro* ( $T_{80}$ ) (Figure 146 1). Each *in vitro* release profile was fitted to a Weibull function prior to the ER predictions.



Figure 1. Mean *in vitro* release profiles for the extended-release drug products of the model drugs with fast (blue), medium (red & purple), and slow (green) release rates, which were used in the predictions after fitting to a Weibull function.

# 152 Investigated absorption models

153 GastroPlus® 9.8.1

GastroPlus<sup>®</sup> is based on the advanced compartmental absorption and transit (ACAT) model
consisting of nine compartments to mimic the human GI tract. The detailed description of the
model is described elsewhere<sup>50, 51</sup>.

157 In GastroPlus<sup>®</sup>, the absorption of a drug from a compartment is based on **Equation** (2):

158

159 
$$\frac{dM_{i(absorbed)}}{dt} = Ka'_i \times V_i \times (C_{lumen_i} - C_{ent,u_i})$$
(2)

160

where  $dM_{i(absorbed)}/dt$  is the rate of absorption, Ka'<sub>i</sub> is the absorption rate coefficient, C<sub>lumen i</sub> is the concentration in the lumen, C<sub>ent,u i</sub> is the unbound concentration of drug in the enterocyte subcompartment, and *i* indicates a particular compartment<sup>51</sup>. In addition, GastroPlus<sup>®</sup> includes

164	an Absorption Scale Factor (ASF) in its model. The ASF multiplier scales the effective
165	permeability to adjust for variations in surface-to-volume ratio, pH effects, and other
166	absorption rate-determining effects that may vary from one gastrointestinal compartment to
167	another according to <b>Equation (3)</b> :
168	
169	$Ka'_i = ASF_i \times P_i$ (3)
170	
171	where $\mbox{ASF}_i$ and $\mbox{P}_i$ are the absorption scale factor and effective human permeability of the $i^{th}$
172	compartment, respectively <sup>51</sup> . The default Opt LogD V6.1 model was selected and used in this
173	study.
174	
175	
176	
177	GI-Sim 5.6
178	GI-Sim is a mechanistic PBBM software developed within AstraZeneca. The GI-Sim
179	absorption model is divided into nine physiological compartments coupled in series: stomach
180	(1), the small intestine (2-7), and the colon (8-9). The detailed description of each compartment
181	is described elsewhere <sup>52</sup> . The current GI-Sim model considers the unidirectional transfer of
182	uncharged drugs through the intestinal wall. The absorptive flux $(dM/dt)$ is calculated by
183	Equation (4):
184	
185	$\frac{dM_{(absorbed)}}{dt} = A \times P_{mem} \times (C_{lumen} - C_{ent,u}) $ (4)
186	

Where A is the surface area available for absorption,  $P_{mem}$  is the membrane permeability of 187 uncharged molecule,  $C_{lumen}$  is the total drug concentration in the lumen, and  $C_{ent,u}$  is the unbound 188

drug concentration in the enterocyte sub-compartment. The current GI-Sim model has an option enabling drug administration to any of the nine compartments for regional drug absorption investigations as described earlier<sup>24</sup>.

- 192
- 193

# 194 Modelling strategy

195 The overall modeling strategy was to evaluate the prediction performance of three different 196 approaches to account for colon absorption in the prediction of the vivo performance of ER 197 drug product variants of the model drugs. Firstly, an *a priori* approach using the current default 198 colon models was evaluated to reflect an early ER product development scenario when no in 199 vivo understanding exists, e.g., during candidate selection or product design. Secondly, the ASFs or area in the colon model in GastroPlus<sup>®</sup> and GI-Sim, respectively, were optimized to 200 201 fit the mean plasma concentration-time profile observed after direct administration of the drug 202 to the colon to reflect a situation where an early human regional absorption study was 203 performed to generate a mechanistic understanding of the extent of colon absorption. Finally, the ASFs or area in the colon model in GastroPlus<sup>®</sup> and GI-Sim, respectively, were optimized 204 205 to fit the observed mean plasma concentration-time profile of the slowest ER variant for each 206 model drug to mimic a situation where in vivo data of prior ER prototypes are available. The 207 slowest release profile was used since it represents the scenario when the highest fraction is 208 released in the colon, and the colon absorption limitation is the highest. Mechanistic models 209 were developed for the prediction of the relative bioavailability ( $F_{rel}$ ), the area under the curve 210 (AUC<sub>0-t</sub>), and maximum plasma drug concentration (C<sub>max</sub>) for the ER drug product variants in both GastroPlus<sup>®</sup> (ver. 9.8.1003, Simulations Plus Inc., Lancaster, CA) and GI-Sim (ver. 5.6, 211 AstraZeneca). Initially, an intravenous model was developed using PKPlus<sup>®</sup> compartmental 212 modeling in GastroPlus<sup>®</sup>. All simulations were performed using compartmental modeling 213

214 without the addition of any specific enzymes or transporters. Furthermore, it was assumed that 215 no luminal degradation occurred in the GI tract. The compartment model with the best-fitted weighting function, based on lowest value of the Akaike Information Criterion (AIC) and 216 217 Schwarz Criterion (SC), was used to calculate the disposition parameters. The human fasted physiology model with a body weight of 70 kg was used throughout the GastroPlus® 218 219 simulations. Oral immediate-release models for solution and tablet drug products were 220 developed based on the intravenous disposition parameters (except for AZ2, where disposition 221 parameters were calculated based on oral solution data) and the other input parameters (Table 222 1). Lastly, an ER drug product model was developed where three different approaches to account for colon absorption in the predictions were evaluated (Figure 2). 223



**Figure 2.** PBBM strategy for the ER drug products, including the three approaches to account

226 for colon absorption. ASF: Absorption scale factor

227

228

229

#### 231 *a priori prediction approach*

The oral absorption models for either solutions or IR tablets, in combination with *in vitro* release data, were used for model development for each ER drug product variant. No fittings were performed to the observed data in either software package.

235

# 236 Colon absorption approach

237 In the colon absorption approach, the *a priori* developed ER model for each model drug was 238 modified to account for the observed plasma data after direct colon administration of the model 239 drugs generated in the human regional absorption studies. This was done by initially developing a regional colon absorption model for the model drugs as previously described<sup>24</sup>. 240 241 To mimic colon administration in GastroPlus<sup>®</sup>, the transit times of all compartments before the 242 caecum were set to 0.0001 hour, and the percentage of fluid in the stomach and small intestinal 243 compartments changed to 0.001%. In GI-Sim, this was achieved by administering the model 244 drugs directly to the caecum compartment (8). The developed regional colon absorption model for each drug was further optimized with caecum and colon ASFs in GastroPlus<sup>®</sup> to capture 245 the rate and extent of drug absorption through the colon. This was done by using the 246 'Optimization module' of GastroPlus<sup>®</sup>. These adjustments were analogues to adjustments of 247 ASF values in previous publications<sup>22, 42</sup>. The optimized ASF values were then used to predict 248 the *in vivo* plasma exposure of the ER drug product variants for the model drugs. To replicate 249 the GastroPlus® optimization of ASFs in GI-Sim, the area of the caecum and colon 250 251 compartment were modified based on Equation (5):

252

253

$$A_i = ASF_i \times V_i \tag{5}$$

254

where  $A_i$  and  $V_i$  are the area and volume of the i<sup>th</sup> compartment, respectively; the default GastroPlus<sup>®</sup> and GI-Sim volumes used for the caecum (V<sub>8</sub>) and ascending colon (V<sub>9</sub>)

- compartments were 47.49 ml and 50.33 ml, respectively. The new area for the eighth and ninth
  compartments was then used in GI-Sim simulations for each drug (Equation 3). The optimized
  ASFs and calculated new caecum and ascending colon areas for each drug are shown in Table
- 260

3.

261

Table 3. Absorption scale factors and corresponding surface areas for the different approachesto account for colon absorption in the predictions.

		Approach											
Drug	Compartment	a pi	riori	Colon at	osorption	Slowest ER							
-		ASF (G <sup>+</sup> ) (1/cm)	Area (GS) (cm <sup>2</sup> )	ASF (G <sup>+</sup> ) (1/cm)	Area (GS) (cm <sup>2</sup> )	ASF (G <sup>+</sup> ) (1/cm)	Area (GS) (cm <sup>2</sup> )						
Matanalal	Caecum	0.05	28.02	2.23	105.95	0.99	46.81						
Metoprotoi	Colon	0.14	41.77	0.00	0.04	0.37	18.41						
0	Caecum	0.07	28.02	0.28	13.39	0.01	0.38						
Oxprenoioi	Colon	0.17	41.77	0.00	0.00	0.21	10.72						
170	Caecum	0.31	28.02	1.12	53.24	9893	469832						
ALZ	Colon	0.58	41.77	1.88	94.77	0.18	9.16						
A 77.1	Caecum	13.00	28.02	0.07	3.37	9507	451511						
AZI	Colon	25.33	41.77	0.02	1.21	0.01	0.60						
Vincele action	Caecum	0.02	28.02	1.57	74.70	0.21	10.02						
Aimeiagatran	Colon	0.05	41.77	0.00	0.05	0.00	0.02						

264

265

# 266 Slowest ER approach

For the slowest ER approach, the same methodology as for the colon absorption approach was used, but the physiology in the caecum and colon compartments used in the predictions were generated by fitting the ASFs or surface areas to the plasma concentration-time profile of the slowest ER variant for each model drug.

271

272

## 273 Model prediction performance assessment

The predictive performance of the three different approaches was evaluated based on the prediction of the maximum plasma drug concentration ( $C_{max}$ ), the area under the curve (AUC<sub>0</sub>-

276 t), and relative bioavailability ( $F_{rel}$ ) ( $F_{rel} = AUC_{ER}/AUC_{IRreference}$ ) for the different ER drug

277 product variants of the model drugs. The prediction performance was calculated individually

using percent prediction error (%PE) for each ER drug product variant and as the average
absolute prediction error (%AAPE) for each model drug and colon modeling approach
according to Equation 6:

281

282 
$$\%AAPE = \frac{1}{N} \left( \sum_{i}^{n} \left| \frac{\text{predicted}_{i} - \text{observed}_{i}}{\text{observed}_{i}} \right| \times 100 \right)$$
 (6)

283

Also, a visual comparison between observed and predicted plasma concentration-time profiles
was performed to assess the predictive performance qualitatively for all drugs.

Two levels of acceptance criteria were selected for the current ER drug product prediction performance assessment: highly accurate and accurate. An AAPE less than or equal to 20% was set for highly accurate predictions, while an AAPE of 20-50% was set for accurate predictions. Predictions with AAPE > 50% were considered to be poor. The acceptance criteria were justified as the PBBM development was based on independent studies and based on previous investigations considering different stages of drug product development<sup>24, 38, 51</sup>.

292

293

294

295

#### 296 **RESULTS**

The observed and predicted  $C_{max}$ , AUC<sub>0-t</sub>, and  $F_{rel}$  of the investigated ER drug product variants for the three different approaches to account for colon absorption are presented in **Table 4**, and the observed and predicted plasma concentration-time profiles are shown in **Figures 3-7**. The overall prediction accuracy of the different approaches is summarized in **Table 5** and presented in **Figures 8-10**. Metoprolol



302

**Figure 3.** Mean ( $\pm$ CV) observed (symbols) and predicted (solid lines) plasma concentrationtime profiles of the three Metoprolol ER drug product variants with different *in vitro* release rates (T<sub>80</sub> of 12, 16, and 25 hours) in GastroPlus<sup>®</sup> (blue) and GI-Sim (red). The *a priori*, colon absorption, and slowest ER approaches are displayed on the top, middle, and bottom rows, respectively.

Oxprenolol







315

**Figure 5.** Mean ( $\pm$ CV) observed (symbols) and predicted (solid lines) plasma concentrationtime profiles of the three AZ2 ER drug product variants with different *in vitro* release rates (T<sub>80</sub> in 6, 11, and 16 hours) in GastroPlus<sup>®</sup> (blue) and GI-Sim (red). The *a priori*, colon absorption, and slowest ER approach are displayed on the top, middle, and bottom rows, respectively.



Figure 6. Mean observed (symbols) and predicted (solid lines) plasma concentration-time profiles of the three AZ1 ER drug product variants with different *in vitro* release rates ( $T_{80}$  in 14, 16, and 22 hours) in GastroPlus<sup>®</sup> (blue) and GI-Sim (red). The *a priori*, colon absorption, and slowest ER approach are displayed on the top, middle, and bottom rows, respectively.

Ximelagatran



326 327 Figure 7. Mean (±CV) observed (symbols) and predicted (solid lines) plasma concentrationtime profiles of the three Ximelagatran ER drug product variants with different in vitro release 328 rates (T<sub>80</sub> in 2, 5, and 10 hours) in GastroPlus<sup>®</sup> (blue) and GI-Sim (red). The *a priori*, colon 329 330 absorption, and slowest ER approach are displayed on the top, middle, and bottom rows, 331 respectively.

332



Figure 8. Overall prediction performance of  $F_{rel}$ , AUC<sub>0-t</sub>,  $C_{max}$ , and  $T_{max}$  for the three different approaches to account for colon absorption in the predictions of the *in vivo* performance of the ER drug product variants for the model drugs in GastroPlus<sup>®</sup> (blue) and GI-Sim (red). Solid and dotted lines represent the line of unity and a 2-fold difference, respectively.



**Figure 9.** Prediction error of  $C_{max}$ , AUC<sub>0-t</sub>, and  $F_{rel}$  for the three approaches to account for colon absorption in the predictions of the *in vivo* ER drug product performance in relation to the assigned colon absorption limitation risk for the model drugs in GastroPlus<sup>®</sup> (blue) and GI-Sim (red). The dotted lines represent the predefined criteria for highly accurate (AAPE $\leq$ 20%) and accurate (AAPE 20%-50%) predictions.

- 346
- 347
- 348
- 349
- 350

# **Table 4.** Observed and predicted human absorption and plasma pharmacokinetic parameters for the ER drug product variants of the model drugs

		Formulation	Observed values			Predicted values																	
						a priori				Colon absorption						Slowest ER							
Drug	Dose		C <sub>max</sub> (ug/ml)	AUC <sub>0-t</sub> (µg.h/ml)	F <sub>rel</sub> (%)	C <sub>max</sub> (µg/ml)		AUC <sub>0-t</sub> (µg.h/ml)		F <sub>rel</sub> (%)		C <sub>max</sub> (µg/ml)		AUC <sub>0-t</sub> (µg.h/ml)		F <sub>rel</sub> (%)		C <sub>max</sub> (µg/ml)		AUC <sub>0-t</sub> (µg.h/ml)		F <sub>rel</sub> (%)	
						$\mathbf{G}^{+}$	GS	G+	GS	$\mathbf{G}^{+}$	GS	$\mathbf{G}^{+}$	GS	G+	GS	$\mathbf{G}^{+}$	GS	G+	GS	G+	GS	$\mathbf{G}^{+}$	GS
	95	Solution	0.1228	1.086	100	0.109	0.1276	0.9783	1.127	100	100												
Metoprolo153		ER T <sub>80</sub> :12h	0.0483	0.8867	82	0.042	0.0533	0.5734	0.9463	59	97	0.0521	0.0545	0.6659	0.7084	68	72	0.0452	0.0528	0.8118	0.9161	83	94
metoprotor	95	ER T <sub>80</sub> :16h	0.0321	0.7233	67	0.013	0.0402	0.2914	0.8122	30	83	0.0262	0.0341	0.3055	0.5151	31	53	0.0235	0.0367	0.5245	0.7739	54	79
		ER T <sub>80</sub> :25h	0.0273	0.5418	50	0.011	0.0260	0.1992	0.5112	20	52	0.0142	0.0142	0.1591	0.2400	16	25	0.0195	0.0229	0.3878	0.4752	40	49
	105.5	IR tablet	0.6581	2.4135	100	0.9902	1.1810	2.8569	2.8667	100	100												
		ER T <sub>80</sub> :13h	0.1922	3.2492	67	0.2532	0.3591	4.5050	4.6700	78	81	0.2678	0.2486	2.3949	2.1960	42	38	0.2508	0.2690	4.5064	4.3820	78	76
Oxprenolol <sup>49</sup>	2127	ER T <sub>80</sub> :16h	0.2126	3.2712	67	0.2506	0.3041	3.9963	4.1033	70	71	0.2612	0.2421	2.2085	2.0140	38	35	0.2490	0.2355	3.9980	3.8600	70	67
	212.7	ER T <sub>80</sub> :17h	0.2439	3.2312	67	0.2461	0.3371	4.2027	4.3333	73	75	0.2596	0.2409	2.2868	2.0920	40	36	0.2439	0.2489	4.2023	4.0720	73	71
		ER T <sub>80</sub> :22h	0.1998	2.9219	60	0.0954	0.2673	1.8014	3.7517	31	65	0.1004	0.1863	0.9113	1.6760	16	29	0.0949	0.2063	1.8061	3.5180	31	61
	75	Solution	1.7887	5.6875	100	1.7792	1.8160	5.6487	6.5920	100	100												
A 72044		ER T <sub>80</sub> :6h	1.206	7.3068	96	0.6537	0.8682	5.9933	7.514	80	100	0.8241	0.9812	6.5707	7.695	87	102	1.0106	1.153	6.1925	7.306	82	97
AL2	100	ER T <sub>80</sub> :11h	0.6446	5.0902	67	0.3752	0.5618	5.5709	6.872	74	91	0.5667	0.6683	6.1722	7.137	82	95	0.6303	0.7115	5.3828	6.275	71	83
		ER T <sub>80</sub> :16h	0.5142	4.9578	65	0.2818	0.3941	4.6076	5.747	61	76	0.3902	0.4532	5.2866	6.069	70	81	0.3768	0.4245	4.1525	4.883	55	65
	100	IR tablet	0.3192	2.981	100	0.5813	0.6170	2.5538	2.5650	100	100												
A 77 1 44		ER T <sub>80</sub> :14h	0.2757	2.6802	45	0.2751	0.2628	4.7548	3.9780	93	78	0.1410	0.1261	2.5981	2.6650	51	52	0.2658	0.2032	2.9353	2.8150	57	55
AZI	200	ER T <sub>80</sub> :16h	0.2204	2.1389	36	0.2539	0.2200	4.5381	3.6330	89	71	0.0824	0.1003	2.1356	2.2270	42	43	0.2053	0.1381	2.2413	2.2590	44	44
		ER T <sub>80</sub> :22h	0.1331	1.7062	29	0.0992	0.1496	1.2269	2.8060	24	55	0.0684	0.0662	1.4518	1.5220	28	30	0.0992	0.0652	1.2540	1.4100	25	28
	50	Solution	0.1611	0.8304	100	0.1923	0.1459	1.0360	0.8565	100	100												
X7 1 44		ER T <sub>80</sub> :2h	0.0606	0.4434	53	0.0533	0.1309	0.2846	0.7537	73	193	0.0618	0.1363	0.4567	0.6911	117	177	0.0550	0.1261	0.3206	0.5414	82	139
Aimelagatran	50	ER T <sub>80</sub> :5h	0.0528	0.4091	49	0.0257	0.0749	0.1635	0.7857	42	202	0.0381	0.0803	0.3958	0.5373	102	128	0.0269	0.0679	0.2268	0.3517	58	90
		ER T <sub>80</sub> :10h	0.0223	0.1888	23	0.0078	0.0387	0.0527	0.5464	14	140	0.0173	0.0286	0.1935	0.2659	50	68	0.0084	0.0216	0.0866	0.1337	22	34

# 352 for the different approaches to account for colon absorption in GastroPlus<sup>®</sup> & GI-Sim

Table 5. Prediction error (PE, %) for the primary pharmacokinetic parameters for the three different approaches to account for colon absorption

357	in the ER in	vivo performanc	e predictions in	GastroPlus®	and GI-Sim
-----	--------------	-----------------	------------------	-------------	------------

		a priori						Colon absorption							Slowest ER					
Drug	T <sub>80</sub> (h)	GastroPlus <sup>®</sup>			GI-Sim			G	astroPlus	®	GI-Sim			G	astroPlus®		GI-Sim			
		Cmax	AUC <sub>0-t</sub>	Frel	Cmax	AUC <sub>0-t</sub>	Frel	Cmax	AUC <sub>0-t</sub>	Frel	Cmax	AUC <sub>0-t</sub>	Frel	Cmax	AUC <sub>0-t</sub>	Frel	Cmax	AUC <sub>0-t</sub>	Frel	
	12	-13	-35	-28	10	7	18	8	-25	-17	13	-20	-12	-6	-8	1	9	3	15	
Metoprolol	16	-60	-60	-55	25	12	24	-18	-58	-54	6	-29	-21	-27	-27	-19	14	7	18	
Wetopioloi	25	-60	-63	-60	-5	-6	4	-48	-71	-68	-48	-56	-50	-	-	-	-		-	
	AAPE	44	53	48	13	8	15	25	51	46	22	35	28	16	18	10	12	5	16	
	13	32	39	16	87	44	21	39	-26	-37	29	-32	-43	30	39	16	40	35	13	
	16	18	22	4	43	25	6	23	-32	-43	14	-38	-48	17	22	4	11	18	0	
Oxprenolol	17	1	30	9	38	34	12	6	-29	-40	-1	-35	-46	0	30	9	2	26	6	
	22	-52	-38	-48	34	28	8	-50	-69	-73	-7	-43	-52	-	-	-	-	-	-	
	AAPE	26	32	20	50	33	12	30	39	49	13	37	47	16	30	10	18	26	6	
	6	16	10	17	20	2		22	10	0	10	~	6	16	15	1.5	1		1	
	6	-46	-18	-1/	-28	3	4	-32	-10	-9	-19	5	6	-16	-15	-15	-4	0	1	
AZ2	11	-42	9	10	-13	35	30	-12	21	22	4	40	42	-2	0	6	10	23	24	
		-45	-/	-0	-23	10	1/	-24	12	8	-12	22	25	-	-	-	- 7	- 12	- 12	
	AAPE	44	11	11	21	18	19	25	15	15	11	25	24	9	10	10	/	12	12	
	14	0	77	107	-5	/18	73	_/10	_3	13	-54	_1	16	-1	10	27	-26	5	22	
	14	15	112	147	-5	70	97	-4)	-5	17	-54	-1	19	-4	5	27	-20	6	22	
AZ1	22	-25	-28	-17	12	64	90	-49	-15	-3	-50	-11	3	-	-	-	-	-	-	
	AAPE	14	73	90	6	61	87	53	6	11	53	5	13	5	7	24	32	5	22	
																	-			
	2	-12	-36	38	116	70	264	2	3	121	125	56	234	-9	-28	55	108	22	162	
<b>X</b> <sup>2</sup> 1	5	-51	-60	-14	42	92	312	-28	-3	108	52	31	161	-49	-45	18	29	-14	84	
Aimelagatran	10	-65	-72	-39	73	189	509	-22	2	117	28	41	196	-	-	-	-	-	-	
	AAPE	43	56	30	77	117	362	17	3	115	68	43	197	29	36	37	68	18	123	

#### 359 *a priori* prediction of the *in vivo* performance of ER drug product variants

With the *a priori* modelling approach, the current absorption models in GastroPlus® and GI-360 361 Sim were assessed for predicting the C<sub>max</sub>, AUC<sub>0-t</sub>, and F<sub>rel</sub> of ER drug product variants of the 362 model drugs with different in vitro release rates without changing any colon physiology 363 parameters. The predefined criteria for accurate predictions (AAPE 20-50%) were met for the 364 low-medium colon absorption risk drugs for all primary prediction parameters (Figures 8-9, **Table 5**), except for the metoprolol GastroPlus<sup>®</sup> predictions, which were borderline to accurate. 365 In predicting C<sub>max</sub>, AUC<sub>0-t</sub>, and F<sub>rel</sub> for the low-medium colon absorption risk drugs, the AAPE 366 range was 11-53% and 8-59% for GastroPlus<sup>®</sup> and GI-Sim, respectively (Table 5). 367 368 Qualitatively, the predicted plasma concentration-time profiles were generally within the 369 interindividual variability for metoprolol and oxprenolol while less well predicted for the low 370 solubility model drug AZ2, especially for the slower ER variants (Figures 3-5). In contrast, 371 the criteria for accurate predictions were not met for the high colon absorption risk drugs AZ1 372 and Ximelagatran (Figures 6-7 and 9, Table 5), resulting in poor qualitative predictions of the 373 mean plasma concentration-time profiles. For the high colon absorption limitation risk drugs, the AAPE range was 14-90% and 6-362% for GastroPlus® and GI-Sim, respectively. By 374 combining all prediction parameters for the *a priori* approach, 36% of the predictions were 375 376 categorized as highly accurate, 33% as accurate, and 31% as poor predictions in GastroPlus<sup>®</sup>, while the corresponding values for GI-Sim were 38%, 33%, and 29% (Figure 10). 377



**Figure 10.** Percentage-distribution of the degree of accuracy of predicted pharmacokinetic parameters ( $C_{max}$ , AUC<sub>0-t</sub>, and  $F_{rel}$ ) combined into highly accurate, accurate, and poor for the *a priori*, colon absorption, and slowest ER approaches to account for colon absorption in the prediction of the ER drug product variants using GastroPlus<sup>®</sup> and GI-Sim.

385 Predictive performance of ER drug product variants with the colon absorption approach 386 The colon absorption approach aimed to evaluate the prediction performance of the ER drug 387 product variants when the observed plasma exposure from a human regional colon absorption study was accounted for in the PBBM development. Using this approach, the prediction 388 389 performance remained unchanged compared to the *a priori* approach, and the predefined 390 criteria for accurate predictions were met for the low-medium colon absorption limitation risk drugs (Figure 8-9, Table 5). There was no obvious/significant change in the prediction 391 392 performance for the high colon absorption limitation risk drugs either (Figure 8-9, Table 5). Qualitatively, the predicted plasma concentration-time profiles for metoprolol and oxprenolol 393 394 were within the observed interindividual variability but with a clear tendency toward

395 underprediction at the later time points, while the prediction of the plasma concentration-time 396 profiles for the solubility/dissolution limited drug AZ2 was slightly improved compared to the 397 a priori approach (Figures 3-5). For the high colon absorption limitation risk drugs, the 398 predictions of the plasma concentration-time profiles were not improved for the 399 solubility/dissolution limited AZ1, while an improvement was seen for the permeability-400 limited drug ximelagatran (Figures 6-7). In predicting C<sub>max</sub>, AUC<sub>0-t</sub>, and F<sub>rel</sub> for low-medium colon absorption risk drugs, the AAPE range was 13-51% and 11-47% for GastroPlus<sup>®</sup> and 401 402 GI-Sim, respectively (**Table 5**). On the other hand, for the high colon absorption limitation risk drugs, the AAPE range was 3-115% and 5-197% for GastroPlus® and GI-Sim, respectively. 403 404 By combining all prediction parameters for the colon absorption approach, 40% of the 405 predictions were categorized as highly accurate, 39% as accurate, and 21% as poor predictions 406 in GastroPlus<sup>®</sup>, while the corresponding values for GI-Sim were 35%, 42%, and 23% (Figure 407 10).

408

# 409 **Predictive performance of the ER drug product variants with the slowest ER approach**

410 For the slowest ER approach, the observed plasma exposure for the slowest ER drug product 411 variant was utilized to account for colon absorption in the ER predictions of the model drugs. 412 With this approach, the prediction performance was significantly improved for all model drugs compared to the *a priori* approach, and the vast majority of the predictions of C<sub>max</sub>, AUC<sub>0-t</sub>, and 413  $F_{rel}$  met the predefined criteria for high accuracy (PE $\leq 20\%$ ) in both GastroPlus<sup>®</sup> and GI-Sim 414 415 (Figure 3-9, Tables 4-5). In predicting C<sub>max</sub>, AUC<sub>0-t</sub>, and F<sub>rel</sub> for all model drugs, except for the permeability-limited drug ximelagatran, the AAPE range was 9-30% and 5-26% for 416 GastroPlus<sup>®</sup> and GI-Sim, respectively (**Table 5**). Qualitatively, the mean plasma 417 418 concentration-time profiles were well predicted for all ER drug product variants of all drugs 419 except for Ximelagatran. By combining all prediction parameters for the slowest ER variant

420 approach, 64% of the predictions were categorized as highly accurate, 33% as accurate, and
421 3% as poor predictions in GastroPlus<sup>®</sup>, while the corresponding values for GI-Sim were 58%,
422 33%, and 9% (Figure 10).

423

424

#### 425 **DISCUSSION**

426 The main objective of this work was to evaluate how well PBBM could predict the in vivo 427 performance of ER drug product variants with different *in vitro* release profiles by using three 428 different approaches to account for colon absorption in the model development. The rationale 429 for this approach was that it is well-established that sufficient colon absorption is a key determinant for successful ER development<sup>1, 6, 7</sup>, and the necessity to apply different PBBM 430 431 approaches at different stages in drug product development. In predictions of ER drug product 432 performance during candidate profiling, product design, and early product development, 433 represented by the *a priori* approach in this evaluation, the prediction accuracy relies on the 434 general prediction performance of the model using default model settings and *in vivo* predictive 435 input parameters since clinical in vivo data is not available. As the early ER PBBM applications 436 mainly include predictions of potential colon absorption limitations, providing initial proof-of-437 concept ER predictions to support the high-level formulation strategy as well as defining the 438 initial *in vitro* ER release target profile, it is appropriate to assign lower predictive performance 439 requirements of the model at this stage. Since mechanistic human regional absorption studies, 440 where the study drug is administered directly to the colon, can be performed to enable early 441 clinical colon absorption and ER development suitability assessments, the "colon absorption 442 approach" evaluated the predictive performance when the colon absorption data generated in 443 such studies was accounted for in the model development. Finally, the evaluation of the prediction performance for the "slowest ER approach" reflected a scenario at a later stage in 444

445 the drug product development process when *in vivo* data on ER prototypes is available and can 446 be accounted for in the colon model of ER predictions. For the latter two approaches, it is 447 appropriate to assign higher prediction performance requirements of the model given the availability of in vivo data to inform model development, especially for commercial drug 448 449 products and regulatory PBBM applications. Availability of PBBMs with stage-appropriate 450 accuracy in the prediction of the *in vivo* performance of ER drug products would provide 451 opportunities to reduce product development time, and cost since the selection of candidate 452 drugs, the decision to initiate development or not, as well as a definition of target release 453 profiles and in vitro release methods would be greatly facilitated. Accurate PBBMs would also 454 reduce the need for clinical relative bioavailability studies. The results demonstrated that, in 455 relation to the predefined prediction performance criteria, the *a priori* approach was sufficiently 456 accurate to be used to predict the *in vivo* performance of ER drug products during candidate 457 selection and early product design and development for low and medium colon absorption 458 limitation risk drugs. In addition, the "slowest ER approach" significantly improved the 459 prediction performance and provided the opportunity to use this methodology for ER PBBM 460 development for commercial drug products and regulatory applications, except for low 461 permeability drugs. In contrast, the "colon absorption" approach did not improve the prediction 462 performance compared to the *a priori* approach.

463

The results also showed that the prediction performance for the *a priori* approach did not meet the predefined criteria for highly accurate prediction. This is in agreement with a recently published evaluation of the ability of PBBM to predict regional and colon absorption in humans, where accurate predictions were achieved for high permeability drugs while the prediction performance was poor for low permeability drugs<sup>24</sup>. The relatively poor predictions of the plasma concentration-time profiles for the ER drug product variants of the low 470 permeability compound ximelagatran and the borderline high permeability compound metoprolol in both GastroPlus<sup>®</sup> and GI-Sim and in GastroPlus<sup>®</sup>, respectively, are also in 471 agreement with the previous evaluation, where it was shown that GastroPlus<sup>®</sup> underpredicted 472 while GI-Sim overpredicted the colon absorption of low permeability drugs<sup>24</sup>. The fact that all 473 474 ER drug product variants of all model drugs displayed various degrees of regional dependent 475 absorption as indicated by the lower F<sub>rel</sub> observed compared to the IR reference formulation. 476 This demonstrates that PBBM of ER drug products will always be more complex than the IR 477 counterpart for the same compound. Based on this, it was not surprising that highly accurate 478 predictions were not achieved with the *a priori* approach. Furthermore, the results highlighted 479 that more efforts are needed to develop more mechanistically and physiologically based colon 480 models to achieve highly accurate *a priori* predictions of the *in vivo* performance of ER drug 481 products.

482

483 Human regional absorption studies where the study drug is administered directly to the colon 484 have been used to assess the extent of colon absorption and guide decisions to initiate ER drug 485 product development<sup>7</sup>. Recently, the colon absorption data generated in these studies have been 486 used to establish in vivo predictive in vitro models to enable colon absorption limitation assessments already during candidate selection<sup>7, 23</sup>. Interestingly, accounting for the observed 487 488 plasma exposure after direct colon administration in the colon models did not improve the 489 prediction performance. It seems that the colon ASFs generated for the low colon absorption 490 limitation risk drugs metoprolol and oxprenolol predicted the initial part of the ER plasma 491 concentration-time profiles well, while the later part was underpredicted. This can be explained 492 by the fact that these compounds are rapidly and completely absorbed within a limited region 493 after a bolus dose to the colon, whereas an ER drug product is released and absorbed through 494 a broader region of the colon. In contrast, the colon ASFs derived for the dissolution/solubility 495 limited compounds AZ2 and AZ1 predicted the relative bioavailability of the ER drug product 496 variants well, but the predicted absorption rate was slower than the observed. The colon 497 absorption approach surprisingly predicted the ER drug product variants with 5 and 10h release 498 profiles of the low permeability drug ximelagatran. The likely explanation for this is that the 499 permeability rather than the release from the drug product variants determines the absorption 500 rate, which is well captured by the colon ASFs generated based on data after a bolus dose to 501 the colon. All in all, there seems to be a limited value in performing human regional absorption 502 studies where the drug is administered to the colon as a bolus to support PBBM development 503 for ER drug products. On the other hand, it should be stressed that the application of telemetric 504 capsule techniques where the drug content is released at a defined rate throughout the 505 gastrointestinal tract would likely be beneficial in PBBM development and predictions of ER drug products. 506

507

For the "Slowest ER approach", the extracted ASFs from the plasma concentration-time 508 509 profiles of the slowest ER drug product variants seemed to capture all the key factors related 510 to permeability, dissolution, and release throughout the colon, which resulted in significantly 511 improved predictions compared to the *a priori* approach for all model drugs regardless of colon 512 absorption limitation risk. Even though this approach did not meet the high accuracy criteria in 513 all cases, it should be considered as a very promising methodology to achieve highly predictive 514 compound specific PBBMs qualifying for commercial and regulatory applications until highly 515 accurate *a priori* models are available. This approach also presents opportunities to reduce 516 product development time and costs, which includes opportunities to reduce the number or 517 streamline the design of relative bioavailability studies. Since this evaluation aimed to directly 518 compare the three different approaches to account for colon absorption in the predictions of the 519 *in vivo* performance of the ER drug product variants, the number of suitable model drugs were 520 limited. Therefore, an additional evaluation with a larger dataset could be considered to gain 521 further confidence in the predictive performance using the slowest ER approach. A limited 522 dataset of drugs with distinct biopharmaceutics properties and different degrees of colon 523 absorption limitation risks was included in this evaluation, which needed to be taken into 524 consideration in the justification of the selected prediction performance parameter and 525 acceptance criteria. Therefore, it was decided to treat the selected drugs as separate case studies 526 rather than a complete dataset, which also warranted the selection of %AAPE as the prediction performance parameter in line with traditional IVIVC development<sup>54</sup>. Furthermore, the 527 528 assigned acceptance criteria for accurate predictions were considered appropriate for a model 529 at an early product development stage in line with the prediction performance criteria applied for other pharmacokinetic parameters at this stage of development<sup>24, 55</sup>. The assigned criteria 530 531 of AAPE less than or equal to 20% for highly accurate predictions, which reflected a prediction 532 performance sufficient to predict the in vivo performance of an ER drug product from a 533 commercial drug product applications perspective, differs from the 10% criteria applied in traditional IVIVC development<sup>54</sup>. However, in this evaluation, the developed mechanistic 534 535 models utilized data from several different clinical studies compared to traditional IVIVC, 536 where the clinical data is generated in a single cross-over study. Moreover, in this evaluation 537 the ER drug product variants used in the predictions spanned across a significantly wider in 538 vitro release and pharmacokinetic parameter range than the 10% difference recommended for 539 traditional IVIVC development, which is more challenging from a regional absorption 540 prediction perspective. Based on this, it was considered appropriate to assign AAPE  $\leq 20\%$  as 541 the criteria for highly accurate predictions in this evaluation.

542

Finally, the importance of the selection and development of an appropriately biorelevant and
discriminatory *in vitro* release/dissolution method for successful PBBM development for ER

545 drug product predictions should be emphasized since a wrongly selected dissolution method could lead to failed PBBM<sup>56</sup>. The selection should be made in close collaboration between *in* 546 vitro dissolution and biopharmaceutics scientists, and a framework for key considerations in 547 the selection of an *in vitro* dissolution method has been described previously<sup>56</sup>. A successful 548 549 PBBM development will establish a link between the *in vitro* release rate, ideally the quality 550 control (QC) dissolution method, and the clinical in vivo performance for the ER drug product, 551 which potentially will allow instant acceptance or rejection of manufactured batches, enable 552 clinically relevant release specifications, and waive in vivo studies during product development 553 and for post-approval changes. In the current study, we assumed that discriminatory and 554 potentially biorelevant dissolution method was used to generate the data and same was used as 555 an input in the PBBM. Moreover, there is a need for a more mechanistic way to incorporate 556 the dissolution data of ER drug products like product particle size distribution (P-PSD) as available for IR drug products<sup>57, 58</sup>. Additionally, the volume of fluid available in colon 557 558 compartments, hydrodynamics, luminal degradation, binding of drugs to fecal or luminal 559 contents, and mucus diffusion are some of the critical parameters for ER drug product 560 performance where clarity is still needed. A comprehensive systematic evaluation of each 561 parameter independent of the other could help to understand these grey areas.

562

#### 563 CONCLUSION

The physiologically based biopharmaceutics modeling of ER drug products with *a priori* modeling demonstrated sufficient accuracy for low-medium colon absorption limitation risk drugs enabling use during candidate selection and early product development. The results also indicate a limited value in performing human regional absorption studies where the drug is administered to the colon as a bolus to support PBBM development for ER drug products. Instead, performing an early streamlined relative bioavailability study with the slowest relevant

570	ER in vitro release profile may develop a highly accurate PBBM suitable for ER predictions
571	for commercial applications, except for permeability-limited drugs.
572	
573	Corresponding Author
574	Christer Tannergren: Oral Product Development, Pharmaceutical Technology &
575	Development, AstraZeneca Gothenburg, S-431 83 Mölndal, Sweden.
576	Email: christer.tannergren@astrazeneca.com
577	
578	ACKNOWLEDGMENT
579	This publication has received funding from the European Union's Horizon 2020 research and
580	innovation programme under the Marie Skłodowska-Curie grant agreement No 956851.
581	
582	DECLARATION OF INTEREST
583	H.J. and C.T. are both employees of AstraZeneca. GI-Sim has been developed by AstraZeneca
584	for internal and academic use. AstraZeneca has ongoing license agreements for GastroPlus <sup>®</sup> .

# 586 **REFERENCES**

587 1. Thombre, A. G., Assessment of the feasibility of oral controlled release in an 588 exploratory development setting. *Drug discovery today* **2005**, *10* (17), 1159-1166.

589 2. Chien, Y., Fundamentals of controlled-release drug administration. *Novel Drug*590 *Delivery System Marcel Dekker, New York* 1982, 465-574.

591 3. Wilding, I.; Coupe, A.; Davis, S., The role of γ-scintigraphy in oral drug delivery.
592 Advanced drug delivery reviews 2001, 46 (1-3), 103-124.

- 593 4. Abdul, S.; Poddar, S., A flexible technology for modified release of drugs: multi layered 594 tablets. *Journal of controlled release* **2004**, *97* (3), 393-405.
- 595 5. EMA, Guideline on the pharmacokinetic and clinical evaluation of modified release 596 dosage forms. European Medicines Agency London: 2014.
- 6. Abuhelwa, A. Y.; Foster, D. J. R.; Upton, R. N., A Quantitative Review and Metamodels of the Variability and Factors Affecting Oral Drug Absorption—Part II:
  Gastrointestinal Transit Time. *The AAPS Journal* 2016, *18* (5), 1322-1333.
- Tannergren, C.; Bergendal, A.; Lennernäs, H., *et al.*, Toward an increased
  understanding of the barriers to colonic drug absorption in humans: implications for early
  controlled release candidate assessment. *Molecular pharmaceutics* 2009, *6* (1), 60-73.
- 8. Jamei, M.; Abrahamsson, B.; Brown, J., *et al.*, Current status and future opportunities for incorporation of dissolution data in PBPK modeling for pharmaceutical development and regulatory applications: OrBiTo consortium commentary. *European Journal of Pharmaceutics and Biopharmaceutics* **2020**, *155*, 55-68.
- 607 9. Dahlgren, D.; Roos, C.; Lundqvist, A., *et al.*, Regional Intestinal Permeability of Three
  608 Model Drugs in Human. *Molecular pharmaceutics* 2016, *13* (9), 3013-21.
- 10. Diakidou, A.; Vertzoni, M.; Goumas, K., *et al.*, Characterization of the contents of
  ascending colon to which drugs are exposed after oral administration to healthy adults. *Pharmaceutical research* 2009, 26 (9), 2141-51.
- 612 11. Schiller, C.; Fröhlich, C. P.; Giessmann, T., *et al.*, Intestinal fluid volumes and transit
  613 of dosage forms as assessed by magnetic resonance imaging. *Alimentary pharmacology &*614 *therapeutics* 2005, 22 (10), 971-9.
- 615 12. Wilson, C. G., The transit of dosage forms through the colon. *International journal of* 616 *pharmaceutics* **2010**, *395* (1-2), 17-25.
- 617 13. Vertzoni, M.; Augustijns, P.; Grimm, M., *et al.*, Impact of regional differences along
  618 the gastrointestinal tract of healthy adults on oral drug absorption: An UNGAP review.
  619 *European journal of pharmaceutical sciences : official journal of the European Federation for*620 *Pharmaceutical Sciences* 2019, *134*, 153-175.
- 14. Tannergren, C.; Borde, A.; Boreström, C., *et al.*, Evaluation of an in vitro faecal
  degradation method for early assessment of the impact of colonic degradation on colonic
  absorption in humans. *European journal of pharmaceutical sciences : official journal of the European Federation for Pharmaceutical Sciences* 2014, 57, 200-6.
- 15. Vertzoni, M.; Carlsson, A.; Abrahamsson, B., *et al.*, Degradation kinetics of
  metronidazole and olsalazine by bacteria in ascending colon and in feces of healthy adults. *International journal of pharmaceutics* 2011, *413* (1-2), 81-6.
- 628 16. Sousa, T.; Paterson, R.; Moore, V., *et al.*, The gastrointestinal microbiota as a site for 629 the biotransformation of drugs. *International journal of pharmaceutics* **2008**, *363* (1-2), 1-25.

- 630 17. Söderlind, E.; Abrahamsson, B.; Erlandsson, F., *et al.*, Validation of the IntelliCap®
  631 system as a tool to evaluate extended release profiles in human GI tract using metoprolol as
  632 model drug. *Journal of Controlled Release* 2015, *217*, 300-307.
- Bithavala, Y. K.; Heizer, W. D.; Parr, A. F., *et al.*, Use of the InteliSite® capsule to
  study ranitidine absorption from various sites within the human intestinal tract. *Pharmaceutical research* 1998, *15* (12), 1869-1875.
- Vinarov, Z.; Abrahamsson, B.; Artursson, P., *et al.*, Current challenges and future
  perspectives in oral absorption research: An opinion of the UNGAP network. *Advanced Drug Delivery Reviews* 2021, *171*, 289-331.
- 639 20. Martinez, M. N.; Mochel, J. P.; Neuhoff, S., *et al.*, Comparison of Canine and Human
  640 Physiological Factors: Understanding Interspecies Differences that Impact Drug
  641 Pharmacokinetics. *The AAPS Journal* 2021, *23* (3), 1-16.
- Barmpatsalou, V.; Dubbelboer, I. R.; Rodler, A., *et al.*, Physiological properties,
  composition and structural profiling of porcine gastrointestinal mucus. *European Journal of Pharmaceutics and Biopharmaceutics* 2021, *169*, 156-167.
- Kesisoglou, F.; Balakrishnan, A.; Manser, K., Utility of PBPK absorption modeling to
  guide modified release formulation development of gaboxadol, a highly soluble compound
  with region-dependent absorption. *Journal of pharmaceutical sciences* 2016, *105* (2), 722-728.
- 648 23. Sjögren, E.; Abrahamsson, B.; Augustijns, P., *et al.*, In vivo methods for drug 649 absorption–comparative physiologies, model selection, correlations with in vitro methods 650 (IVIVC), and applications for formulation/API/excipient characterization including food 651 effects. *European Journal of Pharmaceutical Sciences* **2014**, *57*, 99-151.
- 4. Tannergren, C.; Jadhav, H.; Eckernäs, E., *et al.*, Physiologically Based
  Biopharmaceutics Modeling of regional and colon absorption in humans. *European Journal of Pharmaceutics and Biopharmaceutics* 2023, *186*, 144-159.
- Abend, A.; Heimbach, T.; Cohen, M., *et al.*, Dissolution and translational modeling
  strategies enabling patient-centric drug product development: the M-CERSI workshop
  summary report. *The AAPS Journal* 2018, 20 (3), 60.
- Parrott, N.; Suarez-Sharp, S.; Kesisoglou, F., *et al.*, Best practices in the development
  and validation of physiologically based biopharmaceutics modeling. A workshop summary
  report. *Journal of Pharmaceutical Sciences* 2021, *110* (2), 584-593.
- 27. Yuvaneshwari, K.; Kollipara, S.; Ahmed, T., *et al.*, Applications of PBPK/PBBM
  modeling in generic product development: an industry perspective. *Journal of Drug Delivery Science & Technology* 2022, 103152.
- 664 28. Anand, O.; Pepin, X. J.; Kolhatkar, V., *et al.*, The use of physiologically based 665 pharmacokinetic analyses—In biopharmaceutics applications-regulatory and industry 666 perspectives. *Pharmaceutical research* **2022**, *39* (8), 1681-1700.
- 667 29. Gray, V. A.; Mann, J. C.; Barker, R., *et al.*, The case for physiologically based
  668 biopharmaceutics modelling (PBBM): what do dissolution scientists need to know. *DissoTech*669 2020, *12*, 14.

30. Madny, M. A.; Deshpande, P.; Tumuluri, V., *et al.*, Physiologically Based
Biopharmaceutics Model of Vildagliptin Modified Release (MR) Tablets to Predict In Vivo
Performance and Establish Clinically Relevant Dissolution Specifications. *AAPS PharmSciTech* 2022, 23 (4), 108.

Heimbach, T.; Kesisoglou, F.; Novakovic, J., *et al.*, Establishing the bioequivalence
safe space for immediate-release oral dosage forms using physiologically based
biopharmaceutics modeling (PBBM): case studies. *Journal of pharmaceutical sciences* 2021, *110* (12), 3896-3906.

- 32. Wu, D.; Li, M., Current State and Challenges of Physiologically Based
  Biopharmaceutics Modeling (PBBM) in Oral Drug Product Development. *Pharmaceutical research* 2022, 1-16.
- 681 33. FDA, The Use of Physiologically Based Pharmacokinetic Analyses —
  682 Biopharmaceutics Applications for Oral Drug Product Development, Manufacturing Changes,
  683 and Controls Guidance for Industry. DRAFT GUIDANCE. 2020.
- Abend, A.; Heimbach, T.; Cohen, M., *et al.*, Dissolution and Translational Modeling
  Strategies Enabling Patient-Centric Drug Product Development: the M-CERSI Workshop
  Summary Report. *Aaps j* 2018, 20 (3), 60.
- 687 35. Heimbach, T.; Suarez-Sharp, S.; Kakhi, M., *et al.*, Dissolution and Translational
  688 Modeling Strategies Toward Establishing an In Vitro-In Vivo Link-a Workshop Summary
  689 Report. *Aaps j* 2019, 21 (2), 29.
- 690 36. Mitra, A.; Parrott, N.; Miller, N., *et al.*, Prediction of pH-Dependent Drug-Drug
  691 Interactions for Basic Drugs Using Physiologically Based Biopharmaceutics Modeling:
  692 Industry Case Studies. *J Pharm Sci* 2020, *109* (3), 1380-1394.
- Mitra, A.; Suarez-Sharp, S.; Pepin, X. J., *et al.*, Applications of physiologically based
  biopharmaceutics modeling (PBBM) to support drug product quality: a workshop summary
  report. *Journal of Pharmaceutical Sciences* 2021, *110* (2), 594-609.
- 696 38. Riedmaier, A. E.; DeMent, K.; Huckle, J., *et al.*, Use of Physiologically Based
  697 Pharmacokinetic (PBPK) Modeling for Predicting Drug-Food Interactions: an Industry
  698 Perspective. *Aaps j* 2020, 22 (6), 123.
- Suarez-Sharp, S.; Cohen, M.; Kesisoglou, F., *et al.*, Applications of Clinically
  Relevant Dissolution Testing: Workshop Summary Report. *Aaps j* 2018, *20* (6), 93.
- 40. Darwich, A. S.; Margolskee, A.; Pepin, X., *et al.*, IMI–Oral biopharmaceutics tools
  project–Evaluation of bottom-up PBPK prediction success part 3: Identifying gaps in system
  parameters by analysing In Silico performance across different compound classes. *European*Journal of Pharmaceutical Sciences 2017, 96, 626-642.
- 41. Eckernäs, E.; Tannergren, C., Physiologically Based Biopharmaceutics Modeling of
  Regional and Colon Absorption in Dogs. *Molecular pharmaceutics* 2021, *18* (4), 1699-1710.
- Jereb, R.; Opara, J.; Legen, I., *et al.*, In vitro–In vivo Relationship and Bioequivalence
  Prediction for Modified-Release Capsules Based on a PBPK Absorption Model. *AAPS PharmSciTech* 2020, 21 (1), 1-11.

43. Lukacova, V.; Woltosz, W. S.; Bolger, M. B., Prediction of modified release
pharmacokinetics and pharmacodynamics from in vitro, immediate release, and intravenous
data. *The AAPS journal* 2009, *11* (2), 323-334.

44. Sjögren, E.; Westergren, J.; Grant, I., *et al.*, In silico predictions of gastrointestinal
drug absorption in pharmaceutical product development: application of the mechanistic
absorption model GI-Sim. *European journal of pharmaceutical sciences : official journal of the European Federation for Pharmaceutical Sciences* 2013, 49 (4), 679-98.

Fredlund, L.; Winiwarter, S.; Hilgendorf, C., In Vitro Intrinsic Permeability: A
Transporter-Independent Measure of Caco-2 Cell Permeability in Drug Design and
Development. *Molecular pharmaceutics* 2017, 14 (5), 1601-1609.

46. Lennernäs, H., Intestinal permeability and its relevance for absorption and elimination. *Xenobiotica; the fate of foreign compounds in biological systems* 2007, *37* (10-11), 1015-51.

- 47. Eriksson, U. G.; Bredberg, U.; Hoffmann, K.-J., *et al.*, Absorption, distribution,
  metabolism, and excretion of ximelagatran, an oral direct thrombin inhibitor, in rats, dogs, and
  humans. *Drug metabolism and disposition* **2003**, *31* (3), 294-305.
- Rowland, M.; Benet, L. Z.; Graham, G. G., Clearance concepts in pharmacokinetics. *Journal of pharmacokinetics and biopharmaceutics* 1973, *1* (2), 123-136.
- 49. Langenbucher, F.; Mysicka, J., In vitro and in vivo deconvolution assessment of drug
  release kinetics from oxprenolol Oros preparations. *British Journal of Clinical Pharmacology* **1985**, *19* (S2), 151S-162S.
- Agoram, B.; Woltosz, W. S.; Bolger, M. B., Predicting the impact of physiological and
  biochemical processes on oral drug bioavailability. *Advanced drug delivery reviews* 2001, *50*,
  S41-S67.
- 51. Davies, M.; Jones, R. D. O.; Grime, K., *et al.*, Improving the Accuracy of Predicted
  Human Pharmacokinetics: Lessons Learned from the AstraZeneca Drug Pipeline Over Two
  Decades. *Trends in pharmacological sciences* 2020, *41* (6), 390-408.
- 52. Sjögren, E.; Westergren, J.; Grant, I., *et al.*, In silico predictions of gastrointestinal
  drug absorption in pharmaceutical product development: application of the mechanistic
  absorption model GI-Sim. *European journal of pharmaceutical sciences* 2013, 49 (4), 679698.
- 53. Sandberg, A.; Abrahamsson, B.; Sjögren, J., Influence of dissolution rate on the extent
  and rate of bioavailability of metoprolol. *International journal of pharmaceutics* 1991, 68 (13), 167-177.
- Food and Drug Administration, Guidance for industry: extended release oral dosage
  forms: development, evaluation, and application of in vitro/in vivo correlations. US
  Department of Health, H. S., Center for Drug Evaluation & Research, Ed. 1997.
- 55. Davies, M.; Jones, R. D. O.; Grime, K., *et al.*, Improving the Accuracy of Predicted
  Human Pharmacokinetics: Lessons Learned from the AstraZeneca Drug Pipeline Over Two
  Decades. *Trends in Pharmacological Sciences* 2020, *41* (6), 390-408.

749 56. Flanagan, T.; Mann, J., Dissolution universal strategy tool (DUST): a tool to guide 750 dissolution method development strategy. Dissolution Technologies 2019, 26 (3), 6-17.

Pepin, X. J. H.; Flanagan, T. R.; Holt, D. J., et al., Justification of Drug Product 751 57. 752 Dissolution Rate and Drug Substance Particle Size Specifications Based on Absorption PBPK 753 Modeling for Lesinurad Immediate Release Tablets. Molecular pharmaceutics 2016, 13 (9), 754 3256-3269.

755 58. Takano, R.; Furumoto, K.; Shiraki, K., et al., Rate-Limiting Steps of Oral Absorption 756 for Poorly Water-Soluble Drugs in Dogs; Prediction from a Miniscale Dissolution Test and a 757 Physiologically-Based Computer Simulation. Pharmaceutical research 2008, 25 (10), 2334-758 2344.

759

#### 760 **GRAPHICAL ABSTRACT**



762

763

764

765